From Appendage to Crosslinker – Unusual Swelling Behavior in Spiropyran-Modified Hydrogels

Michael M. Lerch,^{1,2,#,*} Ankita Shastri,^{3,#} Thomas B.H. Schroeder,¹ Amos Meeks,¹ Shucong Li,³ Anna V. Shneidman,¹ Michael Aizenberg,¹ Joanna Aizenberg^{1,3,*}

- ¹ John A. Paulson School of Engineering and Applied Sciences, Harvard University, Cambridge, MA 02138, USA;
- ² Stratingh Institute for Chemistry, University of Groningen, Nijenborgh 7, 9747 AG, Groningen, The Netherlands;
- ³ Department of Chemistry and Chemical Biology, Harvard University, Cambridge, MA 02138, USA; # equal contributions
 - * corresponding authors: * jaiz@seas.harvard.edu & *mlerch@seas.harvard.edu

Abstract

Stimuli-responsive materials typically contain responsive molecular units that couple an external trigger to a defined macroscale response. Ongoing efforts to boost the versatility and complexity of these responses increasingly focus on multi-stimuli-responsive molecular units and crosslinkers, as these bear the potential to impart self-regulatory behaviors building on cooperative effects and feedback mechanisms. Herein, we study a stimuli-responsive platform consisting of polyacrylamide-based hydrogels with well-known multi-responsive spiropyrans covalently bound as pendant groups or 'non-innocent' crosslinkers. Surprisingly, as compared to their appended counterparts, spiropyran crosslinkers cause up to two-fold larger hydrogel swelling in methylenebisacrylamide-crosslinked poly(acrylamide-co-acrylic acid) hydrogels, despite their increased relative crosslinking density. We seek the origin of this unexpected behavior by employing nanoindentation, swelling studies, and UV-vis spectroscopy to study changes in mechanical properties and in spiropyran isomer distribution as a function of solution pH, comonomer chemistry, and swelling-induced polymer strain. We then estimate the osmotic counterion pressures as a function of spiropyran isomer distribution but find that such pressures alone are insufficient to explain the observed behavior. Charge complexation, cooperative effects between the hydrogel's mechanics and chemistry, and aggregate formation may all be invoked to explain features of the observed 'non-innocence' of spiropyran crosslinkers. Taken together, these insights will aid rational implementation of such responsive crosslinkers in materials design and extend the functionality of existing polymeric materials towards more complex and better tunable behaviors.

Introduction

Stimuli-responsive hydrogels are crosslinked polymer networks with high water content that undergo large and precisely tunable volume changes in response to physical and chemical stimuli.¹ Such hydrogels can be engineered to absorb or expel water upon a change in humidity, temperature, pH, electric field, illumination, or other stimuli. The degree of volume changes at both the local and the global level within the hydrogel can be pre-programmed by judiciously choosing the network architecture, backbone chemistry, dopants, and chemical and entropic driving forces.^{2–5} The ease of fabrication, chemical versatility, and degree of tunability of responses have led to the pervasive adoption of stimuli-responsive hydrogels as size-changing smart materials,⁶ with applications spanning a vast range, including microfluidics,^{7–9} soft robotics,^{4,5,10} 4D printing,^{11,12} optical components,¹³ soft bioelectronics,^{14,15} drug release platforms,¹⁶ and cell culture scaffolds.^{17,18}

Many stimuli-responsive hydrogels have by now been developed, but most employ a network architecture whereby the responsive group is attached to the polymer chain as an appendage.^{19,20} However, opportunities to engineer more complex dynamic behaviors arise when responsive moieties are employed as 'non-innocent' crosslinkers^{21,22} that connect polymer chains, as such architectures couple chemical changes to network dynamics and *vice versa*. Spiropyrans^{23–27} (**Fig. 1a**) constitute ideal candidates for such crosslinkers because they can exist as isomers with vastly different physical and chemical properties, and thus isomerization greatly affects the local hydrogel network; simultaneously, as spiropyrans are responsive to multiple classes of stimuli, including mechanical strain,^{28,29} polymer swelling can, in turn, impose shifts in chemical equilibrium that influence the molecules' sensitivity to other inputs and that feed back into the polymer network.

Spiropyrans isomers exhibit starkly differing geometry, polarity, dipole moment, charge, acidity,^{30,31} absorption, and fluorescent properties (**Fig. 1a**). The stability of these isomers strongly depends on their environment and molecular structure,^{23,25,32–34} so the equilibrium between all interconverting isomers can be influenced by pH, solvent polarity,³⁵ temperature,^{36,37} light,³⁸ analytes,³⁹ and mechanical force.^{28,29} In aqueous environments, the polarity of the solvent stabilizes the hydrophilic, strongly colored, ring-open merocyanine form (**MC**) or its protonated analogue (**MCH**⁺), depending on the pH of the environment; yet substantial amounts of the hydrophobic, colorless spiropyran form (**SP**) are still present, particularly at higher pH.^{40,41} The ring-open **MC** and **MCH**⁺ forms can undergo ring-closure to **SP** with visible light or with an increase in hydrophobicity of the surrounding microenvironment. In turn, UV light, heat, or mechanical force can be used to ring-open the **SP** isomer.

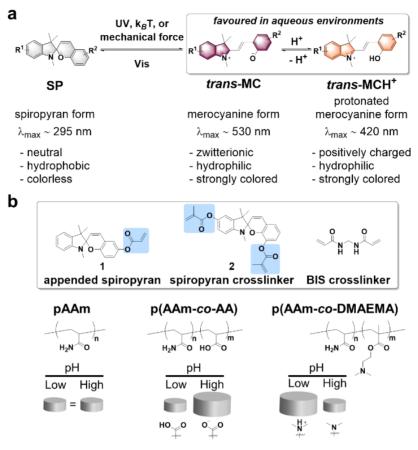


Figure 1. Spiropyran-based hydrogels considered in this work: a) most relevant spiropyran isomers (**SP**, **MC** and **MCH**⁺) and their properties. b) Spiropyrans as an appendage (1) or as a crosslinker (2) were studied in three types of hydrogels with different pH-dependent swelling-behavior: unresponsive pAAm (polyacrylamide), acidic p(AAm-*co*-AA) gels (poly(acrylamide-*co*-acrylic acid)) that swell with higher pH, and basic p(AAm-*co*-DMAEMA) gels (poly(acrylamide-*co*-2-(dimethylamino)ethyl methacrylate)) that swell at lower pH.

For spiropyrans pendant to a hydrogel network, changes in charge, dipole moment, and polarity associated with stimuli-triggered switching between isomers (from **MCH**⁺/**MC** to **SP**) affect the swelling equilibrium of the polymer matrix.¹⁹ Adjustments to the appended spiropyran group's molecular structure and charge are commonly utilized to tailor the swelling behavior of these gels.²⁰ Fixed charges within the hydrogel matrix trigger volume changes in hydrogels because they require mobile counterions, which cause the osmotic pressure of the hydrogel interior to rise. For more non-polar elastomers, in which the ring-closed SP form dominates, incorporating spiropyrans as crosslinkers allows one to use them as mechanophores: mechanically stretching these polymers triggers ring-opening of the non-colored **SP** to the colored **MC** isomer, allowing the ensuing local coloration of the elastomer to function as a strain reporter.^{42,43} Both types of spiropyran behavior are widely used, but the interplay between these (and other) modalities for the creation of self-regulated soft materials has received little attention and remains difficult to

account for when designing smart systems. Here, we provide insights into this interplay of multiple stimuli-responsive modalities of spiropyrans in polyacrylamide-based hydrogels and demonstrate the utility of spiropyrans as non-innocent crosslinkers (**Fig. 1b**). We find that hydrogels equipped with a spiropyran-based crosslinker show *unexpected large-magnitude swelling*, which we attribute to the interplay of mechano-responsivity and pH-responsivity together with an increase in steric constraint around the spiropyran crosslinker. By invoking possible charge complexation effects and cooperativity between the gel's chemical and mechanical properties we provide possible explanations for the observed trends and highlight that non-innocent crosslinkers provide interesting design implications for hydrogel actuators.

Results and Discussion

An unusual swelling behavior

The investigations described herein were triggered by the observation of large increases in hydrogel swelling in spiropyran-crosslinked poly(acrylamide-co-acrylic acid) hydrogels (p(AAmco-AA-co-2), Fig. 2) in the context of our efforts to design optically active, self-regulated hydrogels.^{44,45} To this end, spiropyran variants **1** and **2** were synthesized (**SI Sections 1 and 2**) and co-polymerized into methylenebisacrylamide-crosslinked polyacrylamide hydrogels (SI Section 3, Tables S3.1-S3.3, verification of attachment by FTIR in SI Section 5.1). The spiropyran-free, control hydrogel, p(AAm-co-AA) polymerized at a 1:1 AAm:AA molar ratio and crosslinked with 1.1 mol% methylenebisacrylamide (BIS), swells in aqueous media with a swelling ratio (SR) increasing from ~2 to ~11 as pH increases from pH 5.5 to 7.5, due to the accumulation of negative charges on the polymer backbone resulting from the deprotonation of carboxylic acid moieties ($pK_a \sim 4.7$, Fig. 2, black line). When p(AAm-co-AA) hydrogels are copolymerized with 0.4 mol% spiropyran 1 (Fig. 2, orange line), a similar trend with slightly higher swelling ratios (from ~3 to ~14) above pH 5.5 is observed. Interestingly, when p(AAm-co-AA) hydrogels are copolymerized with 0.4 mol% spiropyran 2 as an additional crosslinker to the 1.1 mol% BIS (Fig. 2, blue line), the resulting hydrogel slabs display dramatically enhanced swelling across the pH range (e.g. ~7 vs. ~3 at pH 5.5 and ~20 vs. ~13 at pH 6.8 for p(AAm-co-AA-co-2) and p(AAm-co-AA-co-1), respectively). This stark increase in swelling ratio is particularly remarkable given the relatively low concentration of spiropyran (0.4 mol%) and that less swelling might be expected at the higher crosslinking density resulting from the presence of an additional crosslinker 2.

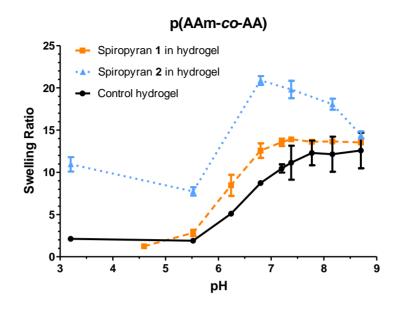


Figure 2. pH-dependent volume change of spiropyran-functionalized p(AAm-co-AA) in 50 mM phosphate buffer, in which spiropyran 1 acts as an appendage and spiropyran 2 as a crosslinker. The swelling ratio (SR) at each pH was calculated as SR = (mass swollen – mass dry)/mass dry.

Hydrogel swelling results from a balance of the elastic pressure of the gel network, which favors collapse, with the solvent mixing and ionic osmotic pressure, which drive gel swelling. Changing the degree of crosslinking within a hydrogel will affect the elastic properties of the gel network and thus the extent of swelling at equilibrium. To confirm the observed effect, we measured swelling and mechanical properties in control pAAm hydrogels (SI Section 4). Non-functionalized pAAm hydrogels are expected to undergo no pH-dependent changes in their charged state; they do not significantly change volume across the examined pH range (Fig. S5.5). Incorporation of spiropyran 2 produces slightly higher swelling ratios across the pH range. We then performed nanoindentation measurements (Fig. S4.1) to estimate the elastic moduli in order to check whether the additional crosslinks provided by 2 are indeed reflected in the mechanics of the gel (Fig. 3, & Figs. S4.2 & S4.3). Comparing pAAm control hydrogels with either 1.1 mol% or 2.2 mol% BIS crosslinker, but no spiropyran, shows, as expected, that swelling decreases by about 21% and the elastic modulus increases as crosslinking density increases by about 37%. Incorporating either spiropyran 1 or 2 significantly decreases the elastic modulus for both 1.1 mol% or 2.2 mol% BIS-crosslinked hydrogels (Fig. 3; by about 63% and 43% for p(AAm-co-1) with either 1.1 mol% or 2.2 mol% BIS, respectively). In addition, p(AAm-co-2) at 1.1 mol% BIS exhibits about a 38% drop in elastic modulus with respect to the pAAm control, but a 66% increase with respect to p(AAm-co-1). This effect persists even after correcting for hydrogel swelling (Fig. **S4.4**), suggesting an effectively lower crosslinking density, which could possibly be explained by inhomogeneities during free radical polymerization. We further note, that the spiropyran

crosslinker is about 1.5-fold or 2.2-fold longer than BIS in its **SP** or **MC** form, respectively, possibly influencing network dynamics in this way. Nevertheless, comparing p(AAm-*co*-AA-*co*-1) and p(AAm-*co*-AA-*co*-2) at 1.1 mol% BIS crosslinking demonstrates that the switch from appendage to crosslinker increases the effective crosslinking density. However, this increase in elastic modulus is not reflected in otherwise expected reduction in swelling, as we observe greater swelling in p(AAm-*co*-AA-*co*-2) compared to p(AAm-*co*-AA-*co*-1).

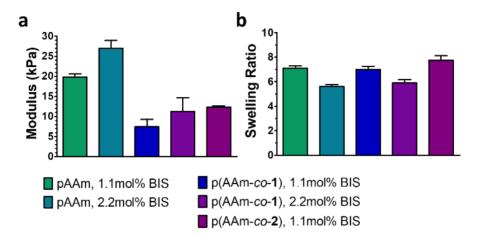


Figure 3. Influence of crosslinking density on elastic moduli and swelling of neutral pAAm hydrogels. a) Elastic moduli of pAAm gels soaked in deionized water measured by nanoindentation. b) Swelling ratio of pAAm gels swollen in PBS 1X pH 7.2.

Stimuli-responsive swelling/contraction for hydrogels with appended spiropyrans relies on changes in charge and polarity between the positively charged **MCH**⁺, zwitterionic (overall neutral) **MC**, and neutral **SP** spiropyran isomers.^{19,20,44} We therefore set out to elucidate the isomer distributions for both spiropyran variants at different pH values in the gel to understand whether the difference in swelling could be explained by differences in isomer distribution (and thus changes in osmotic counterion pressure) alone. To that end, UV-vis spectroscopy was used to identify spiropyran isomer signatures in buffered spiropyran solutions and in hydrogels (**SI section 5.3**) to understand how solution pH, covalent attachment, and hydrogel volume affect spiropyran isomer equilibria. To put the p(AAm-*co*-AA) results in context and to experimentally decouple pH and swelling effects on isomer distributions, we also study neutral polyacrylamide (pAAm) and basic poly(acrylamide-*co*-2-(dimethylamino)ethyl methacrylate) p(AAm-*co*-DMAEMA)) hydrogels (**Fig. 1b**), with no and opposite pH-dependent swelling compared to p(AAm-*co*-AA). We then compare these results to a simple theoretical model⁴⁶ (**SI Section 6**) that estimates isomer distribution at different pH based on Donnan equilibrium theory and compare its estimate of resulting osmotic counterion pressures to experimentally observed swelling (**SI Section 5.2**).

Understanding spiropyran 1 isomer distributions

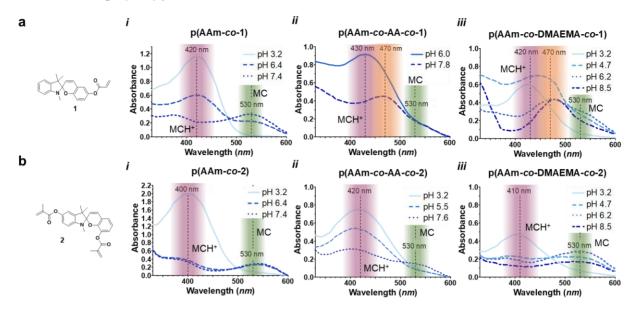


Figure 4. UV-vis spectra of spiropyran-containing hydrogels of different swelling behavior: equilibrium spiropyran isomer distribution for a) spiropyran **1** polymerized into methylenebis(acrylamide)-crosslinked pAAm, p(AAm-*co*-AA), and p(AAm-*co*-DMAEMA) hydrogels in the pH 3-9 range; and b) spiropyran **2** polymerized into methylenebis(acrylamide)-crosslinked pAAm, p(AAm-*co*-AA), and p(AAm-*co*-DMAEMA) hydrogels in the pH 3-9 range; and b) spiropyran **2** polymerized into methylenebis(acrylamide)-crosslinked pAAm, p(AAm-*co*-AA), and p(AAm-*co*-DMAEMA) hydrogels in the pH 3-9 range.

Buffered solutions: We start by determining the pH-dependency of spiropyran isomer distributions in buffered aqueous solutions alone. Compounds **1** and **2** differ in the pK_a of the merocyanine phenolic proton (**MCH**⁺ to **MC** equilibrium); exhibiting an estimated pK_a value of slightly above 6 (**Fig. S5.17**) and 5, respectively. Accordingly, in buffered aqueous solutions (50 mM phosphate buffers), these spiropyrans predominantly exist as the **MCH**⁺ isomer (λ_{max} ~400-430 nm) at low pH and as **MC** (λ_{max} ~530 nm) at high pH (**Figs. S5.15 & S5.16**). Moreover, as pH increases, relatively more **SP** isomer is likely present⁴⁷ as the equilibrium shifts from **MCH**⁺ to **MC** due to **MC**-to-**SP** interconversion. (The absorption band of SP is usually observed below 300 nm and is difficult to resolve in our measurements as reagents and multi-well measurement plates absorb in this region.)

Spiropyran 1 in a neutral hydrogel: We next co-polymerized compound **1** into BIS-crosslinked, neutral pAAm hydrogels immersed within different buffers in order to confirm that covalent attachment to a polymer backbone did not induce changes in the isomerization equilibrium. Indeed, in p(AAm-*co*-**1**) hydrogels, a similar trend was observed as that of free spiropyran in buffer solution (**Fig. 4a**,*i*; **Fig. S5.19**): **MCH**⁺ is present at low pH and converts to **MC** at higher pH. Swelling is comparable for pAAm and p(AAm-*co*-**1**) gels (**Fig. 3b** and **Fig SI S4.3**), indicating that the concentration of charged spiropyran isomers in this neutral gel is not sufficient to induce large swelling effects.

Effect of ionizable co-monomers on spiropyran 1: The presence of acidic or basic comonomers will influence the isomer distribution through ionization and a buffering effect.³³ This effect is evident in pre-polymer solutions (compare Figs. S5.18, S5.21 & S5.24) and crosslinked hydrogels (Fig. 4a,*ii* & 4a,*iii*; Figs. S5.22 & S5.25), where the presence of acrylic acid increases the stability of MCH⁺ to a higher pH (> 6), whereas the basic DMAEMA moieties destabilize MCH⁺ even below pH 5. Because the co-monomer moieties can ionize, their interaction with charged spiropyran isomers may have a stronger effect on hydrogel volume than in the case of neutral pAAm.

Theoretical model: Based on an earlier model,⁴⁶ we implemented a theoretical model based on the Donnan equilibrium to estimate counterion pressures in charged hydrogels as a proxy for swelling (**SI Section 6**). The estimated relative counterion pressures for non-spiropyran functionalized p(AAm-co-AA) and p(AAm-co-DMAEMA) hydrogels fit qualitatively well with experimental results. The internal pH of polyelectrolyte hydrogels is shifted significantly lower (in AA-containing gels) or higher (in DMAEMA-containing gels) compared to the external solution pH (**Figs. S6.3 & S6.7**). Indeed, the swelling at pH 5.5 to 7 for p(AAm-co-AA) hydrogels (control, **Fig. 2**) is induced by the deprotonation of carboxylic acid groups as the gel's internal pH rises above the ~4.7 pK_a of acrylic acid. Similarly, the swelling of p(AAm-co-DMAEMA) gels below pH 7 (**Figs S5.9 & S5.11**) can be correlated with the protonation of the tertiary amine moiety ($pK_a \sim 8.6^{48}$). Potentially, a small amount of hydrolysis of the DMAEMA/AAm co-monomers to AA may contribute somewhat to the experimentally observed gel contraction for DMAEMA-containing gels at lower pH, which is not accounted for by the model. The change in internal pH predicted for nonspiropyran-containing gels also fits well with the experimental shifts in **MCH**⁺ to **MC** equilibrium for both p(AAm-co-AA-co-1) and p(AAm-co-DMAEMA-co-1) gels.

Effect of hydrogel volume change on spiropyran 1: In addition to gel internal pH changes, the hydrogel volume change itself could influence spiropyran isomer distribution, as the microenvironment of the spiropyrans conjugated to the polymer will undergo (*i*) a reduction in the density of surrounding organic molecules, (*ii*) a reduction in the concentration of buffering groups and neighboring spiropyrans, (*iii*) an increase in the size of nearby pores, and (*iv*) an increase in the strain of the polymer network. In order to disentangle these effects, we compared the spiropyran isomer distribution in p(AAm-*co*-AA) and p(AAm-*co*-DMAEMA)—gels with opposite pH-dependent swelling behavior (**Fig. 1b**, **SI Section 5.2**)—keeping in mind the differences in internal pH. p(AAm-*co*-AA-*co*-1) hydrogels show predominantly **MCH**⁺ up to pH 6, similar to the AAm/AA prepolymer solution. In their swollen state at higher pH (pH 7.8, **Fig. 4a**,*ii*; **Fig. S5.22**), these hydrogels exhibit an unexpected absorption band at λ_{max} ~470 nm (for a discussion concerning this peak, *vide infra*). While a shoulder indicative of the **MC** isomer at λ_{max} ~530-540 nm

is observed in the AAm/AA pre-polymer solution (Fig. S5.21) both at low and high pH, no such band is discernible in the polymerized p(AAm-co-AA-co-1) absorption spectrum. For p(AAm-co-DMAEMA) hydrogels, the basicity of the gel disfavors formation of MCH⁺, as can be seen in p(AAm-co-DMAEMA-co-1) hydrogels, in which the **MCH**⁺ isomer is only observed at pH 3.2. As the pH increases to pH 8.5 (dark blue line, Fig. 4a,iii; Fig. S5.25 & S5.26) and the hydrogel contracts, a shift from λ_{max} ~430 nm to λ_{max} ~470 nm is observed. At pH 6.2, an absorption band at λ_{max} ~530 nm is intermittently detectable, possibly indicating presence of the **MC** isomer. Overall, both p(AAm-co-AA-co-1) and p(AAm-co-DMAEMA-co-1) hydrogels favored MCH⁺ at low pH consistent with our model. However, the shift towards an absorption band centered at λ_{max} ~470 nm at higher pH is unexpected and observed for both hydrogels. As these gels swell at opposite pH ranges, the formation of the species identified at λ_{max} 470 nm seems dependent on pH and not on swelling, suggesting that hydrogel volume changes have little effect on the isomer distribution of pendant spiropyrans. With regard to the observed swelling behavior, both hydrogels show slightly increased volumes across the pH range as compared to their non-functionalized counterparts, which is possibly explained by the presence of charged merocyanine isomers to varying degrees at all pH values.

Understanding spiropyran 2 isomer distributions

Next, we turned our attention to hydrogels containing spiropyran 2, which, as a crosslinker, is responsive to mechanical pulling forces from the hydrogel network and thus can serve as a mechanophore, in contrast to compound 1. As hydrogels swell, the network is subjected to swellinginduced strain, which can be released by the ring-opening of the cyclic SP isomer to its merocyanine (**MC/MCH**⁺) counterparts,⁴⁹ possibly changing the isomer distribution. For neutral pAAm hydrogels crosslinked with methylenebisacrylamide and additional spiropyran 2 crosslinker (p(AAm-co-2), Fig. 4b, i; Fig. S5.20), one would expect few changes in spiropyran isomer distribution compared to p(AAm-co-1). Indeed, the MCH⁺ isomer dominates at low pH in favor of the MC-isomer at higher pH. Introduction of the second (meth)acrylate group in spiropyran 2 compared to spiropyran 1 changes the electronics of the system, slightly lowering the effective pK_{a} of the phenolic proton (vide supra, Fig. S5.17), which is particularly apparent in the spectra taken at pH 6.4 (Fig. 4a, i vs. 4b, i). In addition, the altered electronics cause the MCH⁺ absorption band to slightly shift hypsochromically from λ_{max} 420 nm to λ_{max} 400 nm (Figs. S5.15 & S5.16). Nevertheless, experimentally p(AAm-co-2) hydrogels swell more (Fig 3b) in a manner that cannot be explained by the changes in isomer distribution but hints at an explanation invoking other types of effects, as discussed below. P(AAm-co-AA-co-2) hydrogel samples (Fig. 4b, ii; Fig. S5.23) show similar isomer distributions as p(AAm-co-2) (Fig. 4b,i), taking the generally lower internal pH of

p(AAm-*co*-AA) gels (**Fig. S6.3**) and thus later onset of **MCH**⁺ deprotonation into account. As the gel swells with increasing pH, one would expect that strain-promoted ring-opening of **SP** isomers would lead to an increase in charged species in the system, which could further swell the gel (*vide infra*). However, a relative increase in merocyanine isomers is difficult to verify solely from UV-vis spectra.

In order to estimate whether the observed spiropyran isomer distribution for spiropyrans 1 and 2 could be used to explain the changes in swelling trends in p(AAm-co-AA) gels containing spiropyrans shown in Fig. 2, the charges of the different spiropyran isomers were included in our theoretical model (SI Section 6). Estimating counterion pressures in gels containing spiropyran 1 (the model does not include any mechanical effects) suggests, counter to our observations (Fig. 2), that the presence of spiropyran should reduce swelling throughout the pH range but that these effects should be negligible given the low concentration of spiropyran (Figs S6.2 & S6.6). This suggests that the observed swelling trends cannot be simply explained by counterion pressures stemming from charges of spiropyran isomers alone. It is worth noting, that our model assumes spatial homogeneity (*i.e.* perfect charge balance); however, strongly charged polyelectrolytes cause inhomogeneity, 50-53 leading to deviations from the Donnan equilibrium that could contribute to discrepancies between theoretical predictions and experimental results. In addition, for highly swollen (SR>50) and charged polymers, counterion pressures normally dominate, but for lower swelling ratios, as in the present system, mixing pressures have to considered as well.⁵⁴ Therefore, other possible explanations must be considered. We have identified three possible contributors: (i) charge complexation, (ii) cooperative chemo-mechanical effects, and (iii) aggregate formation, which together may explain the observed effects.

Identifying factors contributing to the observed swelling behavior

Charge complexation: Every charged group in a polyelectrolyte solution must be balanced by a counterion of opposite charge. These counterions may be mobile or fixed to a polymer chain. Charge-charge interactions between appended **MCH**⁺ and the deprotonated carboxylic acid in p(AAm-co-AA-co-1) may reduce the mobile counterion pressure at internal pHs between the pK_{as} of **MC** and AA, keeping swelling moderate in this intermediate pH range. For the more sterically hindered spiropyran crosslinker 2 in p(AAm-co-AA-co-2), however, such intermittent charge-charge stabilization may not be possible, thus greatly increasing the mobile counterion pressure (and, in turn, swelling) by comparison. Charge complexation (or lack thereof) can thus be invoked to explain why p(AAm-co-AA-co-1) swells to similar extent to the p(AAm-co-AA) control, but p(AAm-co-AA-co-2) swells much more at low to intermediate pH (**Fig. 2**). This is corroborated by swelling trends in p(AAm-co-DMAEMA) hydrogels (**Figs. S5.9 & S5.11**), in which the positive charge of **MCH**⁺ cannot be counteracted by negative charge from the backbone. An argument against this

explanation is that p(AAm-*co*-AA-*co*-1) hydrogels at 2.2 mol% BIS swell more in this pH range (**Fig. S5.8**), for reasons that remain unclear.

Cooperativity: The dramatic increase in swelling for p(AAm-*co*-AA-*co*-2) hydrogels above pH 5.5 may be a result of chemo-mechanical (in which chemistry controls the mechanics of a material) and mechano-chemical feedback (in which mechanics influences chemistry). As the internal pH increases above the p*K*_a of acrylic acid, p(AAm-*co*-AA-*co*-2) hydrogels swell, inducing ring opening and converting **SP** (which is favored at higher pH⁴⁷) to **MCH**⁺, increasing osmotic pressure and hydrophilicity and causing further swelling (positive feedback). As pH rises further, the **SP/MC/MCH**⁺-isomerization equilibrium shifts away from **MCH**⁺, leading to lower osmotic pressure and some shrinkage. The slight decrease in swelling ratios at higher pH could also be a result of the overall increase in salt concentration in the phosphate buffer solutions,⁵⁰ (**Figs. S5.12, S5.32 & S6.1**). In contrast, for p(AAm-*co*-DMAEMA-*co*-2) hydrogels that swell at low pH, when spiropyran **2** mostly exists as **MCH**⁺, this effect is neither expected nor observed.

Aggregate formation: It is notable that the spiropyran-crosslinked hydrogels (Fig 4b) do not show any formation of the λ_{max} ~470 nm absorption band observed in p(AAm-co-AA-co-1) and p(AAm-co-DMAEMA-co-1). Initial evidence of the possible nature of the species responsible for this absorption band comes from experiments in which p(AAm-co-DMAEMA-co-1) hydrogel volume changes across the pH 3-8 range are suppressed by increasing the salt concentration (200 mM NaCl, Fig. S5.10 & S5.31). Under such conditions, the band at $\lambda \sim 470$ nm is present across the pH range. The 'salting out' effect of increased salt concentration may promote aggregation of the spiropyran appendages in ways that are sterically prevented when spiropyran acts as a crosslinker, thus potentially influencing the swelling behavior of the gels (Fig. 2). Merocyanines are well-known to form H- and J-aggregates. While the MCH⁺ isomer has a generally lower tendency for aggregation, **MC** isomers form blue-shifted H-aggregates with absorption maxima in the range of λ = 440-480 nm. $^{55-57}$ (In p(AAm-co-1) gels, where no additional charges on the backbone are present, that could act as highly concentrated salts and contribute to the 'salting out' effect, no band at λ_{max} ~470 nm is observed.) Aggregated **1-MC** could effectively sequester a significant amount of MC isomers, increasing the hydrophilicity of the polymer backbone and reducing the amount of charge from MCH⁺ that could influence gel swelling. In contrast, spiropyran 2 could be too sterically encumbered to form aggregates and thus have more dye available to enhance swelling. There is also the possibility that such aggregates act as further crosslinking points in the hydrogel, which would reduce swelling, yet the magnitude of such an effect is difficult to estimate. Finally, we note that the presence of spiropyran aggregates may have significant effects on non-linear optical phenomena such as beam-trapping, which are under investigation in our laboratory.44,45

Conclusion

In conclusion, we report that spiropyran crosslinkers in polyelectrolytes can lead to unexpectedly large amounts of swelling compared to equivalent hydrogels with pendant spiropyran moieties. Nanoindentation experiments demonstrate that spiropyran-containing hydrogels have a lower elastic modulus than non-functionalized controls and that employing spiropyran 2 (crosslinker) instead of 1 (appended) increases the relative crosslinking density while also increasing hydrogel swelling. Solution pH, buffering through co-monomers, ionic strength, and polymer strain through hydrogel swelling all influence the isomer distribution of spiropyran, some of which are charged and thus influence counterion pressure and swelling of the gel. However, our results suggest that counterion pressures alone are not sufficient to explain the observed swelling effects. Charge complexation, cooperative effects between mechanical strain and chemical changes in the hydrogel, and aggregate formation may all be invoked to explain features of the observed 'noninnocence' of spiropyran crosslinkers. However, more research will be required to better understand the specific mechanisms by which spiropyran crosslinkers affect hydrogel dynamics. Ultimately, better understanding the origin and role of such phenomena contributes novel insights into the function of an already well-established photoswitch within materials science and provides a new perspective to understand and design dynamic soft materials.

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Author contributions

J.A. and A.S. conceived and initiated the project. A.S. synthesized the spiropyran compounds and hydrogel samples, measured their swelling behavior, mechanical properties, and conducted all UV-visible spectroscopic experiments. M.M.L. conducted follow-up studies to verify observed trends. A.S., M.M.L., T.B.H.S., A.M., M.A., A.V.S., and S.L. performed data analysis and interpretation of results. M.M.L. and J.A. supervised the project. A.S., A.M., T.B.H.S. and M.M.L. wrote the manuscript with contribution from all co-authors. All authors have given approval to the final version of the manuscript.

Competing Interests

The authors declare no competing financial interest.

Supplementary Information

The following supplementary materials are available online:

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